(19) World Intellectual Property Organization International Bureau





(43) International Publication Date 18 November 2004 (18.11.2004)

PCT

(10) International Publication Number WO 2004/098574 A1

(51) International Patent Classification7:

A61K 9/51

(21) International Application Number:

PCT/GB2004/001931

(22) International Filing Date: 5 May 2004 (05.05.2004)

(25) Filing Language:

English

(26) Publication Language:

English

(30) Priority Data:

0310300.9

6 May 2003 (06.05.2003)

- (71) Applicant (for all designated States except US): THE QUEEN'S UNIVERSITY OF BELFAST [GB/GB]; University Road, Belfast BT7 1NN (GB).
- (72) Inventors; and
- (75) Inventors/Applicants (for US only): CRAIG, Duncan, O., M. [GB/GB]; 42 Marlborough Park North, Belfast BT9 6HJ (GB). MC NALLY, John, Anthony [IE/GB]; 11c Lenny's Road, Derryadd, Lurgan, Co Armagh BT66 6QS (GB).
- (74) Agent: MURGITROYD & COMPANY; Scotland House, 165-169 Scotland Street, Glasgow G5 8PL (GB).

- (81) Designated States (unless otherwise indicated, for every kind of national protection available): AE, AG, AL, AM, AT. AU, AZ, BA, BB, BG, BR, BW, BY, BZ, CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DZ, EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, MZ, NA, NI, NO, NZ, OM, PG, PH, PL, PT, RO, RU, SC, SD, SE, SG, SK, SL, SY, TJ, TM, TN, TR, TT, TZ, UA, UG, US, UZ, VC, VN, YU, ZA, ZM, ZW.
- (84) Designated States (unless otherwise indicated, for every kind of regional protection available): ARIPO (BW, GH, GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM, ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European (AT, BE, BG, CH, CY, CZ, DE, DK, EE, ES, FI, FR, GB, GR, HU, IE, IT, LU, MC, NL, PL, PT, RO, SE, SI, SK, TR), OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML, MR, NE, SN, TD, TG).

Published:

- with international search report
- before the expiration of the time limit for amending the claims and to be republished in the event of receipt of amendments

For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

(54) Title: NANOCOMPOSITE DRUG DELIVERY COMPOSITION

(57) Abstract: The invention relates to a drug delivery composition comprising an active ingredient and a biologically inert material wherein the biologically inert material is a nanocomposite material. Preferably the biologically inert material is a polymer-clay nanocomposite comprising up to about 40% by weight of nano-sized (1-1000nm) clay particles dispersed in a polymeric material. The active ingredient may be dispersed in the nanocomposite material or absorbed thereto.

PCT/GB2004/001931 WO 2004/098574

Nanocomposite Drug Delivery Composition

2

1

present invention relates to the use of 3 delivery in drug material nanocomposite 4 compositions. 5

6 It is well recognised that there are a number of 7 circumstances whereby it is desirable to disperse a 8 matrix in biologically inert 9 drug in preparation of a final dosage form. For example, 10 the incorporation of drugs and bioactive molecules 11 solid implants, matrices (eq polymeric 12 into dispersions) has attracted considerable interest as 13 a means of improved drug delivery. Similarly, drug 14 or bioactive-loaded microspheres and nanospheres 15 have received considerable attention. Various drug 16 delivery compositions comprise modified release 17 systems whereby the drug is released at a controlled 18 as to optimise biological activity and 19 drug (eq controlled therapeutic effect of the 20 delivery systems). release oral drug 21 example is the use of drug-loaded medical devices, 22 whereby polymeric devices such as stents may contain 23 antibiotics or anticoagulants for purposes such as 24 the prevention of microbial growth. 25 example is the use of tissue engineering scaffolds, 26 whereby growth factors may be incorporated into a 27 polymeric matrix to optimise cell growth on that 28 In all cases it is necessary to produce 29 matrix. not only release the drug at that systems 30 appropriate rate but also have suitable mechanical 31 properties for the particular application. 32

1

materials that consist of 2 Nanocomposites are particles of one compound with a mean diameter in 3 the nano-size range (1-1000nm) dispersed throughout 4 another material, commonly a modified inorganic clay 5 dispersed within an organic polymer. These polymer-6 clay nanocomposites (PCNs) possess advantageous 7 8 properties compared to the polymer alone such as increased mechanical strength, reduced gaseous 9 permeability and higher heat resistance, even though 10 may be 5% or guantity of clay 11 materials Nanocomposite attracted 12 have interest due to the wide range of alterations in the 13 properties of the base polymer engendered by the 14 incorporation of the clays (see for example Schmidt 15 et al, Current Opin.Solid State Mat.Sci. (2002) 6, 16 205-212; Choi et al, Chem.Mater. (2002) 14, 2936-17 2939; T.J. Pinnavaia and G.W. Beall, "Polymer-clay 18 Chichester, 2001). 19 nanocomposites", Wiley, Moreover, they may be manufactured by a range of 20 techniques using equipment that is well established 21 and hence are economical to produce (depending on 22 the choice of materials, although commonly the 23 materials used are well recognised and inexpensive). 24 25 in drug delivery compositions, 26 The use, potentially useful matrix materials can be limited 27 by their mechanical properties. The matrix must 28 maintain suitable mechanical integrity during the 29 course of the manufacture process and through its 30

subsequent handling and use.

WO 2004/098574 PCT/GB2004/001931

. 3

There are many instances whereby the mechanical 1 properties and / or the release rate of the drugs or 2 bioactives of known drug delivery compositions are 3 The present invention providing as it sub-optimal. 4 does for drug or bioactive-loaded nanocomposites 5 seeks to address these difficulties. 6 7 Therefore, it is an object of the present invention 8 to provide a drug delivery composition wherein the 9 release rate of the drug may be manipulated or 10 altered so as to be optimised for a given drug or 11 application. 12 13 It is another object of the invention to provide a 14 drug delivery composition which is mechanically 15 suitable for the application to which the drug 16 delivery composition is to be put and which is 17 mechanical integrity maintaining of 18 capable throughout the course of its manufacture, storage, 19 handling and use as appropriate. 20 21 It is a further object of the invention to provide a 22 drug delivery composition the manufacture of which 23 economically viable carried out 24 equipment that is readily available. 25 26 Accordingly, the present invention provides for the 27 use of a nanocomposite material in the manufacture 28 of a drug delivery composition. 29 30

31 The invention also provides a drug delivery 32 composition comprising an active ingredient and a

silicones,

31

32

alginates

polymethylmethacrylates,

biologically inert material wherein the biologically 1 nanocomposite material. a material is 2 preferably a polymer-clay nanocomposite. 3 4 is dispersed active ingredient the Preferably 5 throughout a matrix comprising the biologically 6 inert material, although the invention also provides 7 a drug delivery system wherein the active ingredient 8 is loaded in, or adsorbed to, a vehicle comprising 9 the biologically inert material. 10 11 of further provides a method invention 12 The manufacturing a drug delivery composition comprising 13 the steps of forming an admixture comprising a 14 active ingredient and polymer, a clay and an 15 extruding the admixture to produce an extrudate. 16 17 The nanocomposite material may comprise up to about 18 Preferably the polymer 99.9% w/w polymer. 19 present in an amount of from about 90% w/w to about 20 99% w/w of the nanocomposite. 21 22 A wide range of polymers may be employed in the 23 biologically inert material. Examples of suitable 24 polyethylene glycol, poly(εinclude 25 polymers caprolactone), polyvinylpyrrolidone, polylactide, 26 polyethylene, polystyrene, poly(dimethylsiloxane), 27 cellulose polyaniline, polyester, polyimide, 28 derivatives such as hydroxyproyl methyl cellulose 29 ethylcellulose, polysaccharides such as 30 and gelatin, chitosans, and

WO 2004/098574 PCT/GB2004/001931

5

polyacrylonitrile, polyetheretherketone (PEEK), 1 polyamide, polyurethane, bone and dental cements and 2 other polymeric prosthetic materials. In addition 3 such as starch and starch derivatives materials 4 in the would also be suitable for use 5 . Materials that are composed of more than 6 material. one polymer or a polymer and a plasticizer such as 7 polyethylene glycol, water or glycerol may also be 8 9 included. 10 Typically the level of clay within the nanocomposite 11 may range from less than 1% w/w to about 40% w/w, 12 although higher levels may be included. Preferably 13 the amount of clay in the nanocomposite is within 14 the range of from 1% w/w to 10% w/w of 15 nanocomposite material. 16 17 Various clays may be used, either alone or 18 Typically silicates may be used that combination. 19 may be naturally occurring (for example bentonite, 20 montmorillonite and other smectites) or synthetic 21 (for example fluorohectorite, fluoromica, layered 22 double hydroxides). 23 24 nanoparticles clay the of presence 25 The dramatically alter the mechanical properties of the 26 compared invention, of the composition 27 conventional drug delivery vehicle using a polymer-28 only matrix, so as to render the system much more 29 application. The particular for a suitable 30

properties

mechanical

31

32

drug delivery

the

of

composition of the invention may be manipulated by

PCT/GB2004/001931 WO 2004/098574

6

suitable choice of nanocomposite component materials 1 used) and polymers and clays 2 the manufacturing conditions. Furthermore, the rate at 3 which the composition biodegrades may differ from 4 that of the polymer alone and may be tailored to 5 suit a particular active ingredient or therapeutic 6 7 application. 8 The teaching of the invention is applicable to all 9 such methods of nanocomposite manufacture and to all 10 active ingredients (drugs and bioactive materials 11 factors, nutraceuticals, growth 12 including antimicrobials and the like) which can withstand the 13 Suitable manufacturing conditions. drugs 14 bioactives include for example low molecular weight 15 compounds such as indomethacin and paracetamol, 16 compounds such molecular weight 17 higher hydrocortisone, peptides such as cyclosporin A and 18 calcitonin and proteins such as insulin and human 19 The manufacturing method used recombinant DNAse. 20 may be tailored to suit both the performance 21 requirements of the composition and the lability of 22 the incorporated bioactive such that degradation may 23 be minimised by appropriate choice of manufacturing 24 method. 25 26 vary depending on the characteristics of

The amount of active ingredient employed in the drug 27 delivery composition of the present invention may 28 29 particular agent. However, the active ingredient 30 should be employed in an amount which is sufficient 31 to elicit a therapeutic response upon release from 32

WO 2004/098574 PCT/GB2004/001931

7

the drug delivery composition. Typically the active 1 ingredient may be employed in an amount of from less 2 than 1% to about 40% by weight of the composition. 3 4 A drug delivery composition of the invention may be 5 of known method anv to according prepared 6 manufacturing nanocomposites which can be modified 7 so as to facilitate the incorporation of the drugs 8 melt by for example bioactive molecule, 9 or Other manufacturing methods include in 10 extrusion. situ polymerisation (Paul et al, (2003) Polymer, 44, 11 melt intercalation (Lepoittevin et 443-450), 12 (2002) Polymer 43, 4017-4023), sonication (Burnside 13 and Giannelis (1995) Chemistry of Materials, 7, 14 1597-1600) sol-gel technology and solution blending. 15 16 In the case of manufacture by melt extrusion, the 17 may be mixed simultaneously components various 18 (prior to extrusion) in order to disperse the active 19 ingredient throughout the nanocomposite material, 20 although the mixing sequence can influence the 21 product structure and performance and represents 22 another means by which the properties and release 23 the composition characteristics of 24 Other factors such as the choice of 25 controlled. the may influence geometries extrusion screw 26 structure and performance of the extrudate. The 27 drug-loaded nanocomposite extrudate produced may be 28 ground and then formulated into dosage forms such as 29 In such cases, the person tablets and capsules. 30 skilled in the art would appreciate that excipients 31

diluents,

32

such

as

glidants,

lubricants,

disintegrants and the like may be utilised 1 preparation of the final dosage form. 2 modifications known in the field of formulation 3 chemistry, such as the application of enteric or 4 taste masking coatings to tablets for example, may 5 6 be employed. 7 Dosage forms categories for which the invention may 8 be particularly useful include oral drug delivery 9 systems for modified (fast or slow) release, implant 10 non-biodegradable), (biodegradable or 11 microspheres and nanoparticles for oral, 12 parenteral or topical delivery, medical devices, 13 dermatological pessaries, suppositories, 14 preparations, tissue engineering scaffolds. 15 16 The present invention also provides a drug delivery 17 system wherein an active ingredient loaded in, or 18 adsorbed to, a vehicle comprising the biologically 19 inert material, the biologically inert material 20 material. The use nanocomposite 21 being a nanocomposites in the manufacture of drug-loaded 22 medical devices (for example devices such as stents 23 containing antibiotics or anticoagulants) affords 24 similar advantages as those discussed above in terms 25 ingredient delivery controlled active 26 robustness. 27 28

29 Example 1

PCT/GB2004/001931 WO 2004/098574

polyethylene glycol dispersions in 1 Drug nanocomposites for the oral administration of drugs 2 were prepared as follows: 3 4 (Janssen 20000 (PEG) Polyethylene glycol 5 employed polymer the was 6 Pharmaceuticals)

Cloisite 30B (Southern Clay Products, USA) was the 7 clay component. Paracetamol (Sigma, UK) was used as 8 Production οf ingredient. model active 9 nanocomposites was performed by melt extrusion using 10 a Killon KN-100 (Davis Standard Corporation, USA) 11 single screw extruder with rod shaped die (38 mm 12 screw diameter, speed 20-22 rpm, die temp 54-57 °C, 13 temperature zone 1 50 °C - temperature zone 2 55-60 14 °C - temperature zone 3 55-60 °C - temperature zone 4 15 55-60 °C, haul off speed 3-4 m/min, cool to room 16 The powders were not subjected to any temperature). 17

treatments prior to extrusion, other than simple 18 mixing of the three components simultaneously. 19

20

The following combinations were used (all % values 21 are percentages by weight: 22

23

- Paracetamol capsule (number 3, white, gelatin 24 capsule) 25
- 5% paracetamol in PEG (pPEG) 26
- paracetamol 5%/Cloisite 30B 4% /PEG 95% (the 27 drug loaded nanocomposite of the invention) 28

29

The extrudates emerged as cylindrical solid tube-30 like structures of approximately 5 mm in diameter. 31

1cm

32

During the processing of pPEG the following readings 1 were obtained: screw amps: 4; die pressure: 0.1 2 kg/cm²; however when the nanocomposite mixture was 3 extruded the screw amps and die pressure values 4 increased to 8 and 0.4 respectively evidencing the 5 enhanced mechanical strength and resistance of the 6 nanocomposites. Extrusion conditions were optimised 7 by initially heating the system to beyond the 8 melting point of the PEG (circa 60°C) and cooling to 9 circa 56°C so as to extrude the material when in a 10 thus facilitating state supercooled 11 solidification upon extrusion from the equipment. 12 extrudates produced nanocomposite 13 mechanically robust and could be snapped by manual 14 application of pressure. 15 16 In testing the release characteristics of 17 sample the following dissolution methodology was 18 used (Copley DIS 8000): USP apparatus 2 - rotating 19 paddle, 50 rpm; medium - 900 ml deionised water (37 20 °C ± 0.5 °C); analysis - UV spectrophotometer (243 21 22 nm). 23 Dissolution properties were measured as follows: 24 UV calibration plot from a stock solution 25 paracetamol was prepared (100mg in 100ml), with 26 measurements taken at 249nm. Five samples were used 27 for each experiment with 10ml removed at appropriate 28 10mls 37°C intervals and replaced with 29 time deionised water. The samples were analysed using UV 30 Samples were prepared by measurement at 249nm. 31

breaking the extrudate into approximately

- 1 lengths, with a corresponding sample weight of circa
- 2 0.3g. For the pPEG samples, samples were taken
- 3 every 5 minutes for 30 minutes. For the
- 4 nanocomposite composition samples were taken every
- 5 20 minutes for 4 hours.

6

- 7 The release profiles of the three combinations
- 8 tested are shown in Figure 1. The release profile
- 9 of the paracetamol nanocomposite of the invention
- 10 indicates a slower release rate plateauing at about
- 11 60 min compared to rate of release from the
- 12 paracetamol capsule which reached a plateau at about
- 13 30 min. The release profile of the pPEG sample was
- 14 faster that both the drug loaded nanocomposite of
- 15 the invention and the paracetamol capsule,
- 16 plateauing after about 20 min.

17

- 18 The test data indicates that the nanocomposite
- 19 system may be used as a controlled release drug
- 20 delivery system whereby drug release from the
- 21 composition is slowed or otherwise manipulated in
- 22 comparison to the non-clay containing system.

23

24 Example 2

25

- 26 A further drug delivery composition, in the form of
- 27 a drug loaded polyurethane nanocomposite for use in
- 28 an insert device, was prepared as follows:

- 30 The polymer / clay / drug composition was
- 31 thermoplastic polyurethane (95 %) / Cloisite 30B (4
- 32 %) / hydrocortisone (1 %). The mixture of

constituents was extruded using a Collin GmbH twin screw extruder (Model ZK 25), adapter temperature 190 °C, die temperature 19 °C, melt temperature 188 °C, melt zones on the extruder were set between 195 °C and 190 °C from the feed end and screw speed was The mixture was extruded through a cast film die to produce 200 micron thick, 40 to 50 mm wide film of the drug loaded nanocomposite.

32

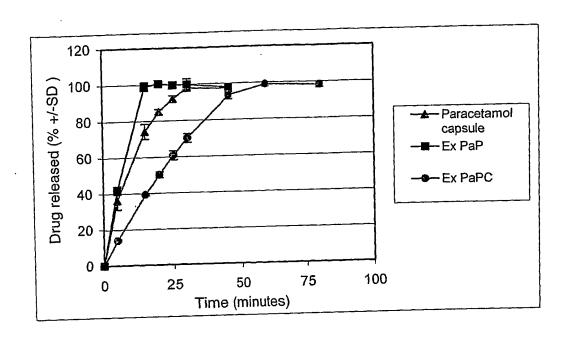
1 2 CLAIMS 3 1. A drug delivery composition comprising an active 4 ingredient and a biologically inert material 5 wherein the biologically inert material is a 6 nanocomposite material. 7 8 2. A drug delivery composition according to Claim 1 9 ingredient is dispersed active wherein the 10 throughout a matrix comprising the biologically 11 inert material. 12 13 3. A drug delivery composition according to either 14 of Claims 1 and 2 wherein the nanocomposite is a 15 polymer-clay nanocomposite. 16 17 4. A drug delivery composition according to any one 18 1 to 3 wherein the nanocomposite ο£ Claims 19 comprises at least one polymer selected from the 20 group consisting of polyethylene glycol, poly(ϵ -21 caprolactone), polyvinylpyrrolidone, polylactide, 22 polystyrene, polyethylene, 23 polyaniline, poly(dimethylsiloxane), polyester, 24 derivatives such cellulose polyimide, 25 hydroxyproyl methyl cellulose and ethylcellulose, 26 polysaccharides such as alginates and chitosans, 27 polymethylmethacrylates, silicones, gelatin, 28 polyacrylonitrile, PEEK, polyamide, polyurethane, 29 cements, starch and dental and 30 derivatives. 31

5. A drug delivery composition according to any one 1 of Claims 1 to 4 wherein the nanocomposite 2 comprises at least one clay selected from the 3 group consisting of bentonite, montmorillonite, 4 fluorohectorite, fluoromica and layered double 5 hydroxides. 6 7 6. A drug delivery composition according to any one 8 of Claims 1 to 5 wherein the amount of clay 9 within the nanocomposite is up to 40% w/w of the 10 nanocomposite material. 11 12 7. A drug delivery composition according to any one 13 of Claims 1 to 5 comprising at least one active 14 ingredient selected form the group consisting of 15 hydrocortisone, paracetamol, indomethacin, 16 cyclosporin A, calcitonin, insulin and human 17 recombinant DNAse. 18 19 8. A drug delivery composition according to any one 20 of Claims 1 to 7 wherein the active ingredient is 21 present in an amount of up to 40% by weight of 22 the drug delivery composition. 23 24 drug delivery system wherein an 9. A 25 ingredient loaded in, or adsorbed to, a vehicle 26 material biologically inert comprising the 27 wherein the biologically inert material 28 nanocomposite material. 29 30

10. A drug delivery system where the nanocomposite material is a polymer-clay nanocomposite.

1	and a second and to either of
2	11. A drug delivery system according to either of
3	Claims 9 and 20 miles
4	comprises at least one polymer selected from the
5	group consisting of polyethylene glycol, poly(ε-
6	caprolactone), polyvinylpyrrolidone, polylactide,
7	polyethylene, polystyrene,
8	poly(dimethylsiloxane), polyaniline, polyester,
9	polyimide, cellulose derivatives such as
10	hydroxyproyl methyl cellulose and ethylcellulose,
11	polysaccharides such as alginates and chitosans,
12	gelatin, polymethylmethacrylates, silicones,
13	polyacrylonitrile PEEK, polyamide, polyurethane,
14	bone and dental cements, starch and starch
15	derivatives.
16	
17	12. A drug delivery system according to any one of
18	Claims 9 and 11 wherein the nanocomposite
19	comprises at least one clay selected from the
20	group consisting of bentonite, montmorillonite,
21	fluorohectorite, fluoromica and layered double
22	hydroxides.
23	
24	13. A drug delivery system according to any one of
25	Claims 9 to 12 wherein the amount of clay within
26	the nanocomposite is up to 40% w/w of the
27	nanocomposite.
28	
29	14. A drug delivery system according to any one of
30	Claims 9 to 13 comprising at least one active
31	ingredient selected form the group consisting of
32	indomethacin, paracetamol, hydrocortisone,

	•
1	cyclosporin A, calcitonin, insulin and human
2	recombinant DNAse.
3	
4	15. A drug delivery system according to any one of
5	Claims 9 to 14 wherein the active ingredient is
6	present in an amount of up to 40% by weight of
7	the drug delivery system.
8	
9	16. A method of manufacturing a drug delivery
10	composition comprising the steps of forming an
11	admixture comprising a polymer, a clay and an
12	active ingredient and extruding the admixture to
13	produce an extrudate.
14	
15	17. A drug delivery composition as defined in any
16	one of Claims 1 to 8 when produced by a method
17	according to Claim 16.
18	
19	18. A drug delivery composition substantially as
20	hereinbefore described.
21	
22	
23	



- ▲ paracetamol capsule
- paracetamol in PEG (pPEG)
- paracetamol loaded nanocomposite of the invention

Figure 1.

INTERNATIONAL SEARCH REPORT

International Application No PCT/GB2004/001931

ı	A. CLASSIF	ICATION O	F SUBJECT	MATTER
	TPC 7	AKIKO	/51	

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

 $\label{eq:minimum documentation searched (classification system followed by classification symbols)} IPC 7 \qquad A61K$

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, WPI Data, PAJ, MEDLINE, EMBASE, BIOSIS, CHEM ABS Data

C. DOCOM	ENTS CONSIDERED TO BE RELEVANT	
Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO 97/13503 A (SELVARAJ ULAGARAJ; MESSING GARY L (US); PENN STATE RES FOUND (US)) 17 April 1997 (1997-04-17) examples 2-5 claims 1,2,4,7,9,15,22	1-18
X	US 2002/164482 A1 (AU MING ET AL) 7 November 2002 (2002-11-07) paragraphs '0006!, '0007!, '0087!, '0090!, '0146!, '0159! claims 1,2,4	1-18
X	US 5 683 719 A (NEWTON JOHN MICHAEL) 4 November 1997 (1997-11-04) example 1 claims 1-3,8,9	16-18

Further documents are listed in the continuation of box C.	Patent family members are listed in annex.
Special categories of cited documents: A' document defining the general state of the art which is not considered to be of particular relevance E' earlier document but published on or after the international filing date C' document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) O' document referring to an oral disclosure, use, exhibition or other means P' document published prior to the international filing date but later than the priority date claimed	 "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art. "&" document member of the same patent family
Date of the actual completion of the international search	Date of mailing of the international search report
13 October 2004	22/10/2004
Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL – 2280 HV Rijswijk Tel. (+31–70) 340–2040, Tx. 31 651 epo nl, Fax: (+31–70) 340–3016	Authorized officer Hedegaard, A

INTERNATIONAL SEARCH REPORT

International Application No
PCT/GB2004/001931

		PC1/GB2004/001931
:(Continua	ation) DOCUMENTS CONSIDERED TO BE RELEVANT	
Category °	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
>,Х	CYPES S H ET AL: "Organosilicate-polymer drug delivery systems: controlled release and enhanced mechanical properties" JOURNAL OF CONTROLLED RELEASE, ELSEVIER SCIENCE PUBLISHERS B.V. AMSTERDAM, NL, vol. 90, no. 2, 24 June 2003 (2003-06-24), pages 163-169, XP004431309 ISSN: 0168-3659 abstract	1-18
4	US 2003/065355 A1 (WEBER JAN) 3 April 2003 (2003-04-03) the whole document	1-18
A	WO 00/34393 A (EASTMAN CHEM CO) 15 June 2000 (2000-06-15) the whole document	1-18

INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No
PCT/GB2004/001931

						7
Patent document dted in search report		Publication date		Patent family member(s)		Publication date
WO 9713503	Α	17-04-1997	EP WO	0862420 9713503		09-09-1998 17-04-1997
US 2002164482	Al	07-11-2002	US US US US US US US US US US US US US	6344271 2003012952 2003012953 2002160190 2002160191 2002168522 2002170593 2002176987 2003207112 2004170820 2004067355 6716525 2004161949 2004180203 2002079476	A1 A1 A1 A1 A1 A1 A1 A1 A1 A1 A1	05-02-2002 16-01-2003 16-01-2003 31-10-2002 31-10-2002 14-11-2002 21-11-2002 21-11-2002 28-11-2002 06-11-2003 02-09-2004 08-04-2004 19-08-2004 16-09-2004 02-05-2002 27-06-2002
US 5683719	A	04-11-1997	AT AU CA DE DE ES FI WO GB HU JP NO ZA	151283 653372 8909691 2096733 69125619 0559813 2101082 932320 9209270 2249957 65756 6502636 931859 9109185	B2 A A1 D1 T2 A1 T3 A A1 A , B A2 T	15-04-1997 29-09-1994 25-06-1992 23-05-1992 15-05-1997 11-09-1993 01-07-1997 09-07-1993 11-06-1992 27-05-1992 28-07-1994 24-03-1994 21-07-1993 30-09-1992
US 2003065355	A1	03-04-2003	CA CA EP EP WO WO US	2456918 2457189 1429833 1429683 03049795 03026532 2003093107	A1 A2 A2 A2 A2	19-06-2003 03-04-2003 23-06-2004 23-06-2004 19-06-2003 03-04-2003 15-05-2003
WO 0034393	Α	15-06-2000	AU AU DE DE EP JP WO US	758915 1935500 69910617 69910617 1141136 2002531675 0034393 6417262 6384121	A D1 T2 A1 T A1 B1	03-04-2003 26-06-2000 25-09-2003 17-06-2004 10-10-2001 24-09-2002 15-06-2000 09-07-2002 07-05-2002

